





Goal: Thalamus nuclear segmentation from random forest learning on MR/DTI - derived multi-modal features.

1. Motivation

- The thalamus is involved in numerous neurodegenerative diseases (Alzheimer's, Multiple Sclerosis, Parkinson's).
- It is composed of neuronal clusters called nuclei, which are responsible for communication between various cerebral cortex and midbrain regions. The nuclei are differentially affected in disease.
- While there is minimal contrast in conventional MR, DTI shows promise (diffusion tensor imaging):
 - Fractional Anisotropy (FA) shows thalamus boundary
 - Changes in Principal Eigenvector (PEV) through Knutsson edge map show inter-nuclear boundaries (see 2.2).
- Others have used spatial location and tensor statistics [Wiegell], connectivity [Behrens], tensor homogeneity [Jonasson, Rittner] to differentiate among nuclei.
- No one has attempted to reproduce manual results without prior information on the target.



and midbrain connectivity



lose-up of example thalamus. Left: in fractional anisotropy (FA), showing the thalamus boundary. Middle: the Knutsson edge map, showing changes in PEV. Right: left thalamus nuclear delineation (manual) from the Knutsson edge map image: anterior nucleus [yellow], medialdorsal [red], ventral group [blue], and pulvinar [orange].

2. Method

- Our goal is to automatically segment the thalamic nuclei using learned patterns in multimodal features. We integrate potentially discriminating features used in prior work, such as spatial coordinates, the Knutsson map, and other DTI-based and structural MRI information.
 - 1. Training: we form a multi-dimensional feature per voxel, which we associate with a nucleus label from a manual rater.
 - 2. Random Forest classification to discriminate thalamus from background and thalamic nuclei from each other, using all the multi-contrast data at our disposal.
 - 3. Target: random forest learners, when applied to a target case, inform the external forces of the MGDM method:
 - > Multiple-object Geometric Deformable Model: level set method enforcing topology constraints [Bogovic].
 - Allows per-boundary forces and object-relative image appearance: nucleus-nucleus, nucleusbackground. This allows the random forest learners to push individual shared boundaries.

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Thalamic Parcellation From Multi-modal Data Using Random Forest Learning

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map and decomposition.

- We integrate 12 potentially discriminating features from structural and diffusion-derived imaging data.
 - **MP-RAGE** (magnetization-prepared rapid acq. with grad. echo) – improved contrast for MS lesions.
 - FA (fractional anisotropy) non-uniformity of diffusion computed using the eigenvalues of the diffusion tensor.
 - MD (mean diffusivity) average eigenvalue of tensor.
 - The PEV is the unit vector associated with the largest eigenvalue of the diffusion tensor. Since opposing vectors in Cartesian coordinates should represent the same orientation, there is a sign ambiguity in defining a difference measure between PEV's. The Knutsson mapping accounts for this ambiguity [Knutsson]: $M([x,y,z]) = \{x^2 - y^2, 2xy, 2xz, 2yz, (2z^2 - x^2 - 2y^2)/\sqrt{3}\}$
 - Knutsson edge map ||G||_F rapidity of change in orientation

Spatial location

MP-RAGE FA



MD

2.3 Random Forest Learning

- Decision trees are constructed through random subsampling of the data and features [Breiman]. Here: single feature, minimum misclassification decision
- Train nucleus-nucleus and nucleus-boundary regions. For each region, output is a tree ensemble that, given a new observation, returns a putative class label for that observation and membership scores for that and the other (less likely) class labels.
- **Test:** apply the ensemble classifiers from the training cases to that subject's data, combining the associated membership scores.





ventral-background



2.2 Feature Selection

Above and right: whole brain axial view of MP-RAGE (top) and Knutsson edge map (right). Below: example vector-valued image (spatial location features not show

M2

M3









ventral-other nuclei

- Unlike previous work, these results were achieved wit requiring extensive prior knowledge of the target's thalamus boundary.



4. Conclusions, Future Directions

- larger number of training cases.



3. Experimental Results

22 MP-RAGE and DTI acquired on 3T MR scanner, resampled to .83mm isotropic

Bagged cross-validation against manual delineations, 10 x train-on-5.

Results exceed previously measured inter-rater variability; while the results on the lateral and medial geniculates are poor, those nuclei are also exceedingly small, potentially only two or three voxels in the original DTI resolution.

7	Nucleus	Mean Dice	Median Dice
out	Anterior	0.576 ± 0.146	0.593
	MedialDorsal	0.641 ± 0.142	0.664
	Ventral Group	0.833 ± 0.074	0.838
	Pulvinar	0.711 ± 0.102	0.725
	Lateral Gen.	0.394 ± 0.202	0.405
	Medial Gen.	0.489 ± 0.244	0.515

Long-term goal is the large scale study of thalamic neuropathology using automated methods. In this paper we have extended thalamic parcellation to place us closer to that goal.

We must improve accuracy, by training more specific (nucleuseverything) random forest learners and pooling results over a

Compare Knutsson to other tensor/PEV dissimilarity measures.

Cortical connectivity to combine global and local information.

Axial view of fiber counts giver seeding within the thalamus. Using FSL Diffusion Toolbox.



Cortical surface colored by region, along with example connectivity-based parcellations of the left thalamus (axial view). These FSL-based results are consistent with those of [Behrens], and show a large variance in parcellation. Note the temporal versus occipital connectivity of the posterior areas.